



# Bone diagenesis in a Mycenaean secondary burial (Kastrouli, Greece)

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## Abstract

This paper presents the characteristics of bone diagenesis in a secondary commingled Mycenaean burial in Kastrouli (Phocis, Greece) through the histological (light microscopy), physical (FTIR-ATR), and biochemical (collagen) analysis of seventeen human (including two petrous bones) and seven animal bones. Post-mortem modifications in bone microstructure, bioapatite, and collagen were characteristic of burial environments with seasonal groundwater and temperature fluctuations. The two human petrous bones displayed a lack of microscopic focal destruction (MFD) sites and a generally good histological preservation, but although a small sample size, did not show any better bioapatite and collagen preservation compared with human femora. Intra-site variations were defined by three main diagenetic patterns that display differences in histological modifications, crystallinity changes, and collagen degradation. These different patterns were either related to different microenvironment conditions and/or influenced by possible differences in the early taphonomic histories experienced by bones prior to secondary deposition. Further, this study highlights the importance of infrared splitting factor (IRSf), carbonate/phosphate ratio (C/P), and general histological index (GHI) for the qualitative assessment of archaeological bone, and the potential use of amide/phosphate ratio (Am/P) as a collagen predictor.

**Keywords** Bone diagenesis · Mycenaean · Secondary burial · Histology · Bioapatite · Collagen

## Introduction

### Bone diagenesis

Bone histology, bioapatite (BAP), and collagen can provide valuable information to the archaeologist and anthropologist.

#### Highlights

- Histological, bioapatite and collagen preservation can vary within 30 cm of sediment.
- Within-site variations may often be related to different funerary treatments.
- Human petrous bones show no microscopic focal destruction.
- Alternating cold-wet and warm-dry cycles lead to the complete destruction of bone.

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Bone histology can be used for the study of the age-at-death, pathology, distinction between human and non-human or burned and unburned bone, etc. (Stout and Teitelbaum 1976; Cattaneo et al. 1999; Mulhern and Ubelaker 2001; Cuijpers 2006; Hanson and Cain 2007; Dominguez and Crowder 2012; De Boer et al. 2013; Assis et al. 2016). Bioapatite is important in archaeological research for the study of past human and animal mobility (strontium and oxygen isotope analyses), dietary habits (carbon isotope analysis), and environments (oxygen isotope analysis) (Lee-Thorp and van der Merwe 1991; Wright and Schwarcz 1996; Hedges 2003; King et al. 2011). Bone collagen is used to determine chronological age (i.e., <sup>14</sup>C dating), past lifeways (e.g., palaeodietary reconstruction, weaning practices), taxonomic identification, and occasionally for screening (e.g., amino acid racemization) (DeNiro and Weiner 1988; Ambrose 1991; Poinar et al. 1996; Collins et al. 1999, 2009; van Klinken 1999; Asara et al. 2007; Buckley et al. 2009; Douka et al. 2017).

The microstructure and the biogenic chemical signals of bone can be altered post-mortem due to bone diagenesis that involves three distinct processes: (a) the microbial attack of bone; (b) the chemical alteration of the inorganic matter (dissolution/recrystallization); and (c) the chemical breakdown of the organic matter (hydrolysis) (Collins et al. 2002; Kendall et al. 2018). Microbial activity can modify bone

microstructure (Hackett 1981; Bell 1990, 2012; Hedges et al. 1995; Turner-Walker and Jans 2008; Hollund et al. 2012; White and Booth 2014; Kontopoulos et al. 2016) and is manifested by microscopic focal destruction (MFD) sites consisting of foci either rounded (linear longitudinal tunneling), branched (budded and Wedl tunneling), or interlinked (lamellate tunneling) that vary from few microns (linear longitudinal tunneling) to hundreds of microns (i.e., lamellate tunneling) in diameter (Hackett 1981).

Microbial attack can also enzymatically degrade collagen using collagenases, with temperature, pH, hydrology, and time also having a profound effect on collagen degradation (Nielsen-Marsh et al. 2000; Grupe et al. 2002; Collins et al. 2002; Koon et al. 2003, 2010; Kendall et al. 2018). Peptide bond hydrolysis and gelatinization activation energies are very temperature sensitive (Collins and Galley 1998) with collagen loss increasing with increasing temperature (Collins et al. 2002; Kendall et al. 2018). Protein hydrolysis in acidic or alkaline environments can also cause fragmentation to collagen and may allow the more soluble components to be leached out as activation energies are also pH dependent (Ajie et al. 1991; Collins and Galley 1998). Local hydrology can also play a significant role in the survival of collagen (i.e., soluble fraction) as bones recovered from warm environments (higher thermal age) may have better preserved organic content than samples of similar chronological age recovered from colder environments (lower thermal age), when the local hydrology is more active (van Doorn et al. 2012).

Any collagen preserved in the archaeological bone presumably can be protected by the bioapatite crystals (BAP) (Grupe 1995) due to their strong *in vivo* relationship (inter-fibrillar and intra-fibrillar deposition of the crystalline material during the mineralization of the organic matrix) (Weiner and Price 1986; Traub et al. 1992; Boskey 2003; Reznikov et al. 2014). The space that is created by the loss of collagen (c. 1/3 of the volume of bone matrix *in vivo*) can be replaced by the growth of the BAP crystals, as a number of ions usually present in the groundwater (e.g.,  $\text{HPO}_4^{2-}$ ,  $\text{PO}_4^{3-}$ ,  $\text{CO}_3^{2-}$ ,  $\text{Ca}^{2+}$ ,  $\text{Mg}^{2+}$ ) can be incorporated into the BAP crystals to create a more ordered and stable crystal environment (Trueman et al. 2004; Lee-Thorp and van der Merwe 1991; Berna et al. 2004; Stathopoulou et al. 2008; Figueiredo et al. 2012; Trueman 2013; Rey and Combes 2014).

The reorganization of the BAP crystals occurs through recrystallization primarily due to active hydrology (Hedges and Millard 1995; Nielsen-Marsh et al. 2000; Hedges 2002) and/or when soil pH is slightly alkaline (c. 7.5–8) (Berna et al. 2004), while recrystallization gives way to dissolution in acidic or alkaline environments (Piepenbrink 1989; High et al. 2015). Therefore, identifying the diagenetic history of each bone can offer unique insight into the preservation potential of bone in different burial environments and timescales, which is of great importance to archaeological, anthropological, and forensic research.

## The Mycenaean secondary burial in Kastrouli

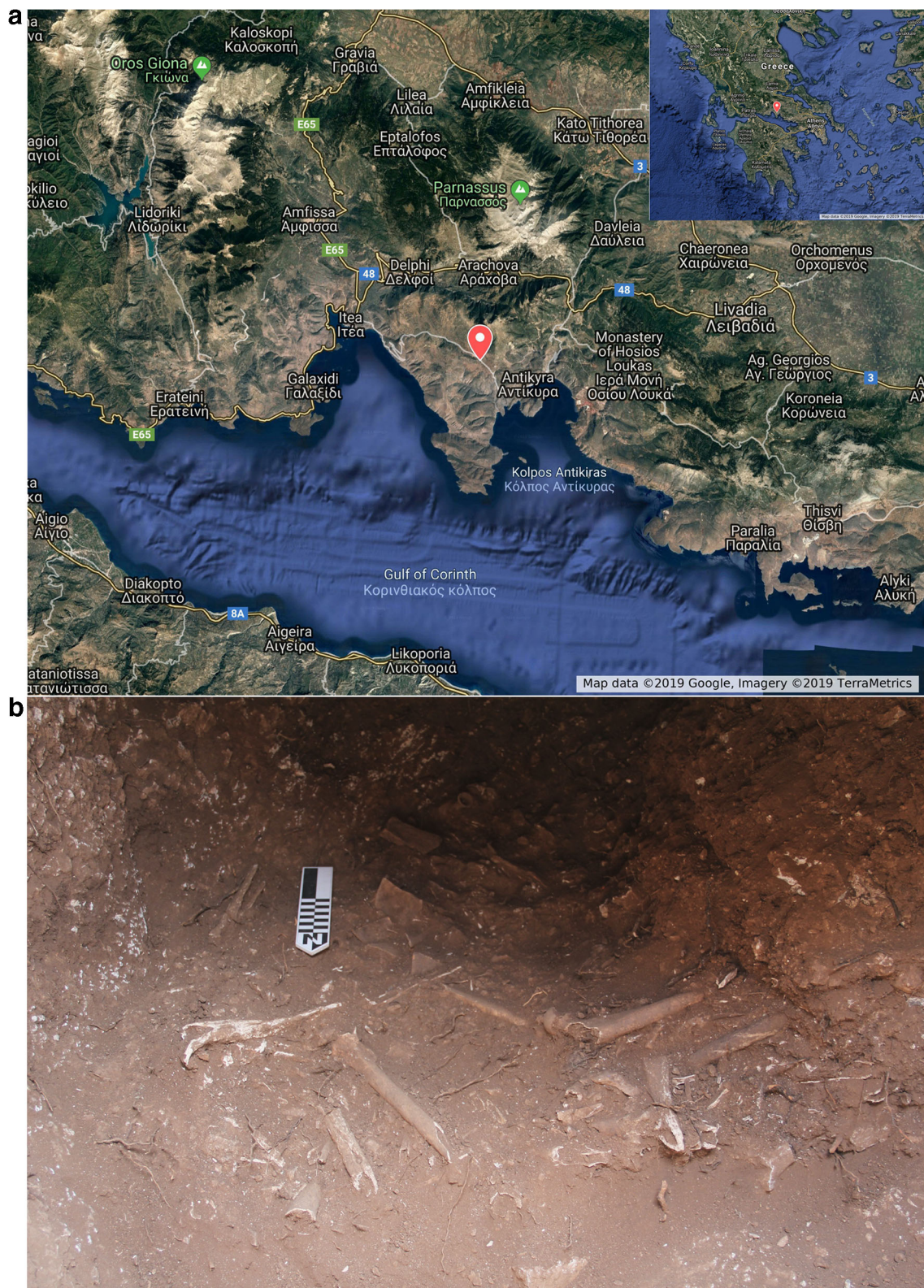
The Mycenaean site of Kastrouli (38.40 N, 22.57 E) is a fortified hill situated in the Mesokampos plateau of the Desfina peninsula (Phocis, Greece) at c. 550 m above sea level, and its position between the Itea and Antikira gulfs was strategic for the control of the entire Desfina peninsula (Fig. 1a). The site has been systematically excavated since 2016, and among the several interesting finds is an undisturbed commingled secondary burial within a rock-cut and built chamber tomb (Sideris et al. 2017). Secondary burials (i.e., the reburial/deposition of the retrieved human skeletal remains, in the same or different locus, at a later time) (e.g., Schroeder 2001) were a common burial practice during the Mycenaean period in Greece. Nonetheless, the forms of secondary treatment (e.g., single secondary burials vs. extensive commingling, tomb elaboration, adult vs. sub-adult individuals) could vary considerably (e.g., Jones 2014; Moutafi and Voutsaki 2016).

The tomb in Kastrouli, which had a W-E orientation, was partly made of limestone and partly carved into the limestone bedrock, and consisted of a dromos in the W, an entrance with monumental lintel, a small chamber, and a niche or extension on the south side covered with a monumental limestone slab (Sideris et al. 2017). The height of the chamber was c. 1.65 m, and although the upper c. 40 cm of sediment of the tomb was disturbed in antiquity and looted in the past decades, the lower c. 30 cm layer was undisturbed (Fig. 1b).

This layer was filled with macroscopically poorly-preserved commingled human bones (minimum number of fifteen adult individuals, two subadults, an infant, and a fetus), alongside numerous pottery fragments, few figurines and beads, few small fragments of gold foil, and a small number of domesticated animal bones (e.g., *Gallus gallus*, *Bos taurus*, *Sus scrofa*, *Ovis aries/Capra hircus*) (Chovalopoulou et al. 2017; Sideris et al. 2017). The bone assemblage was dated on typological grounds of associated ceramic finds to the LH IIIA2–LH IIIC (c. 1350–1150 BC), although a single bone sample (right human femur), residual of the last looting of Tomb A, provided a calibrated  $^{14}\text{C}$  age of 810–760 BC (Liritzis et al. 2016). The Late Mycenaean age of the tomb was also confirmed by the OSL dating of the tomb, the fortified wall, and the ceramics (Liritzis et al. 2019).

The macroscopic analysis of commingled skeletal remains is mainly limited to the minimum number of individuals (MNI), sex, approximate age-at-death, stature, pathology, etc. (Osterholtz et al. 2013; Adams and Byrd 2014). Although the application of other techniques (e.g., optical and scanning electron microscopy, ZooMS, DNA) can potentially answer several important archaeological questions (e.g., human vs. non-human bone, species identification, kinship), such analyses can be obstructed through the partially or totally degraded condition of the skeletal remains (Osterholtz et al. 2013; Adams and Byrd 2014).





**Fig. 1** The strategic position of Kastrouli between the Itea and Antikira Gulfs at the heart of Desfina peninsula (**a**) and the commingled skeletal remains from tomb A (locus 121) found at c. 1 m depth (**b**; scale bar, 1 and 10 cm)

As only a limited number of studies has ever examined bone diagenesis in commingled, disarticulated secondary burials

(e.g., Booth and Madgwick 2016), the aim of this study is to explore the characteristics of bone diagenesis in a secondary



burial environment. Histological (light microscopy), physical (FTIR-ATR), and biochemical (collagen) analyses of human and animal bones were undertaken in order to explore any differences in the diagenetic changes occurred in those commingled archaeological bones. This multi-analytical approach can help elucidate why and how bone degrades in such conditions and shed light on within-site variations possibly related to different primary and secondary funerary treatments.

## Materials and methods

Fifteen human femora, two human petrous bones, and seven animal bones from the Mycenaean site of Kastrouli, Greece were assessed in this study. IBM SPSS v.25 was used for the statistical analysis with the significance level set at  $p = 0.05$ . Regression correlation ( $R^2$ ) is characterized as very weak if it is from 0 to 0.19, weak from 0.2 to 0.39, moderate from 0.40 to 0.59, strong from 0.6 to 0.79, and very strong correlation from 0.8 to 1. These are rather arbitrary bounds and should be considered in the context of the results.

## Histology

Twenty-one transverse thin sections from fifteen human femora and six animal bones, and two longitudinal thin sections from two human petrous bones (Table 1) of c. 200  $\mu\text{m}$  thickness were prepared using an Exact 300 CL diamond band saw. Entellan New (Merck Chemicals) for microscopy was used to mount the undecalcified thin sections onto glass microscope slides cleaned with xylene before use. Thin sections were assessed under a Leica DM750 optical microscope using plane-polarized (PPL) and cross-polarized (XPL) transmitted light at a total magnification ranging from  $\times 40$  to  $\times 400$ . Digital images were captured by a Leica ICC50 HD camera for microscopy imaging with a capture resolution of  $2048 \times 1536$  pixels. The general histological index (GHI) introduced by Hollund et al. (2012) was used as it is comparable with the Oxford histological index (OHI) as described by Millard (2001) but generalized destruction, cracking, and staining are included in the assessment. A GHI value of five represents excellent microstructural preservation similar to modern bone ( $> 95\%$  intact microstructure), whereas a GHI value of 0 indicates poor microstructural preservation ( $< 5\%$  intact microstructure) with almost no original histological features observed.

## FTIR

FTIR-ATR measurements on fifteen human femora, two human petrous bones, and seven animal specimens (Table 1) were performed in triplicate using a Bruker Alpha Platinum (range:  $4000\text{--}400\text{ cm}^{-1}$ ; No. of scans: 144; zero filling factor: 4; resolution:  $4\text{ cm}^{-1}$ ; mode: absorbance). A background

measurement was run before each sample measurement to reduce the background noise and improve the signal-to-noise ratio (SNR). Sample preparation and analysis was carried out according to Kontopoulos et al. (2018). Bone samples were pulverized using an agate pestle and mortar following the mechanical cleaning of the outer and inner bone surfaces. About 2–3 mg of bone powder of 20–50  $\mu\text{m}$  particle size was used for each measurement, and after each measurement, the crystal plate and the anvil of the pressure applicator were thoroughly cleaned using isopropyl alcohol.

The OPUS 7.5 software was used for the calculations of the FTIR indices following: (a) Weiner and Bar-Yosef (1990) for the infrared splitting factor ( $\text{IRSF} = \frac{600\text{ cm}^{-1} + 560\text{ cm}^{-1}}{590\text{ cm}^{-1}}$ ) to assess the BAp crystal size and structural order/disorder, as the larger and/or more ordered crystals display higher IRSF values; (b) Wright and Schwarcz (1996) for the carbonate-to-phosphate ( $\text{C/P} = \frac{1410\text{ cm}^{-1}}{1010\text{ cm}^{-1}}$ ) ratio to detect any diagenetic-related changes to the carbonate content of BAp relative to phosphate content; (c) Sponheimer and Lee-Thorp (1999) for the type B carbonate substitutions relative to phosphate ( $\text{BPI} = \frac{1410\text{ cm}^{-1}}{600\text{ cm}^{-1}}$ ) to detect any diagenetic-related changes to the type B carbonate environment of BAp relative to phosphate content; and (d) Trueman et al. (2004) for the amide-to-phosphate ( $\text{Am/P} = \frac{1640\text{ cm}^{-1}}{1010\text{ cm}^{-1}}$ ) ratio to assess the amount of organic material remaining in the samples relative to phosphate content. The mean values of these indices for two modern human femora and one modern bovine femur were used as reference throughout (Table 1).

For the identification of overlapping/hidden components that cannot be distinguished in the zeroth-order (basic) spectra, derivatization of the spectral curves was carried out (Talsky 1994; Kus et al. 1996; Mark and Workman Jr 2003). The distinction of the overlapping components of the broader amide I band, the  $\nu_2$  and the  $\nu_3\text{ CO}_3^{2-}$  bands through 2<sup>nd</sup> derivative analysis was conducted using the OriginPro 2017 software. The Savitzky-Golay filter was applied to decrease the noise, and a polynomial order of 4 with 13 smoothing points were used for the analysis of the amide I bands and the  $\nu_2\text{ CO}_3^{2-}$  bands (Gander and von Matt 1993; Schafer 2011). As the method is sensitive to noise, a further increase in the number of smoothing points to 25 was applied to the  $\nu_3\text{ CO}_3^{2-}$  band to reduce noise (Kus et al. 1996). Although smoothing reduces the noise, it requires careful consideration as it can also distort the spectral features (Kus et al. 1996).

## Collagen

Collagen was extracted from fifteen human femora, two human petrous bones, and seven animal specimens (Table 1) using a modified Longin (1971) method. The exterior surfaces of the bone samples were mechanically cleaned using a scalpel. Bone chunks of 300–500 mg were demineralized in 8 ml 0.6 M HCl at  $4^\circ\text{C}$ . Samples were agitated twice daily and the acid solution

**Table 1** Summary of data (infrared splitting factor (IRSF); carbonate-to-phosphate (C/P); carbonate type B-to-phosphate index (Am/P); amide-to-phosphate (Am/P); general histological index (GHI))

Sample	Skeletal element	Species	IRSF	C/P	Am/P	BPI	Calcite	712 cm <sup>-1</sup> absorbance	GHI	Diagenetic pathway	Collagen wt.%	Collagen wt.% estimates <sup>a</sup>	C/N
KAS1	R. femur (P)	Human	5.42 ± 0.05	0.10 ± 0.00	0.01 ± 0.00	0.24 ± 0.00	Present	0.00393	1 <sup>b</sup>	1	2.57	2.93	3.70
KAS2	R. femur (P)	Human	3.49 ± 0.02	0.22 ± 0.01	0.04 ± 0.00	0.45 ± 0.01	Absent	0.00	0 <sup>b</sup>	3	6.68	6.17	3.24
KAS3	R. femur (P)	Human	4.79 ± 0.11	0.16 ± 0.01	0.01 ± 0.00	0.38 ± 0.01	Present	0.00949	0 <sup>b</sup>	3	2.26	3.32	3.27
KAS4	R. femur (P)	Human	3.69 ± 0.02	0.17 ± 0.00	0.04 ± 0.00	0.34 ± 0.00	Absent	0.00	0 <sup>b</sup>	3	7.14	6.11	3.19
KAS5	R. femur (P)	Human	4.15 ± 0.13	0.18 ± 0.02	0.02 ± 0.00	0.41 ± 0.01	Present	0.00394	1 <sup>b</sup>	2	5.48	3.64	3.23
KAS6	R. femur (P)	Human	4.74 ± 0.09	0.11 ± 0.01	0.03 ± 0.00	0.25 ± 0.01	Absent	0.00	0 <sup>b</sup>	2	5.79	4.64	3.29
KAS7	R. femur (P)	Human	5.47 ± 0.09	0.09 ± 0.00	0.01 ± 0.00	0.22 ± 0.01	Present	0.00296	0 <sup>b</sup>	1	0.92	3.05	3.99
KAS8	R. femur (P)	Human	4.14 ± 0.17	0.14 ± 0.02	0.05 ± 0.01	0.29 ± 0.02	Absent	0.00	1 <sup>b</sup>	3	11.29	7.59	3.21
KAS9	R. femur (P)	Human	4.12 ± 0.11	0.13 ± 0.02	0.05 ± 0.00	0.25 ± 0.02	Absent	0.00	0 <sup>b</sup>	3	12.07	7.49	3.21
KAS10	R. femur (P)	Human	4.25 ± 0.07	0.12 ± 0.01	0.05 ± 0.00	0.25 ± 0.01	Absent	0.00	1 <sup>b</sup>	3	9.68	7.53	3.21
KAS11	R. femur (P)	Human	5.33 ± 0.01	0.08 ± 0.01	0.02 ± 0.00	0.18 ± 0.00	Absent	0.00	0 <sup>b</sup>	1	2.86	3.62	3.36
KAS12	R. femur (P)	Human	4.09 ± 0.08	0.20 ± 0.01	0.04 ± 0.00	0.42 ± 0.01	Present	0.00462	0 <sup>b</sup>	3	8.14	6.11	3.21
KAS13	R. femur (P)	Human	3.80 ± 0.16	0.16 ± 0.03	0.04 ± 0.01	0.32 ± 0.03	Absent	0.00	1 <sup>b</sup>	3	11.00	6.41	3.21
KAS14	R. femur (P)	Human	3.37 ± 0.12	0.23 ± 0.03	0.05 ± 0.01	0.45 ± 0.04	Absent	0.00	0 <sup>b</sup>	3	6.59	7.54	3.23
KAS15	R. femur (P)	Human	5.37 ± 0.35	0.11 ± 0.02	0.01 ± 0.00	0.27 ± 0.01	Present	0.00623	1 <sup>b</sup>	1	0.86	3.09	3.63
KAS16	Petrous (L)	Human	4.12 ± 0.12	0.15 ± 0.01	0.04 ± 0.00	0.28 ± 0.02	Absent	0.00	3 <sup>c</sup>	Other	10.47	5.94	3.30
KAS17	Petrous (R)	Human	4.07 ± 0.08	0.16 ± 0.01	0.03 ± 0.00	0.34 ± 0.01	Present	0.00129	3 <sup>c</sup>	Other	10.62	4.98	3.30
KAS18	R. carpometaarpus	Chicken	3.57 ± 0.01	0.18 ± 0.00	0.06 ± 0.00	0.35 ± 0.01	Present	0.00012	0 <sup>b</sup>	2	10.89	8.36	3.26
KAS19	R. carpometaarpus	Chicken	3.60 ± 0.04	0.18 ± 0.01	0.04 ± 0.00	0.38 ± 0.01	Absent	0.00	N/A	N/A	9.21	5.77	3.22
KAS22	Phalanx	Cattle	3.52 ± 0.06	0.25 ± 0.01	0.03 ± 0.00	0.54 ± 0.01	Present	0.00192	0 <sup>b</sup>	2	5.28	5.30	3.27
KAS23	L. humerus (D)	Pig	3.61 ± 0.04	0.25 ± 0.01	0.04 ± 0.00	0.48 ± 0.01	Present	0.00200	1 <sup>b</sup>	2	7.70	6.11	3.23
KAS26	R. calcaneus	Cattle	4.10 ± 0.24	0.16 ± 0.03	0.01 ± 0.00	0.33 ± 0.04	Absent	0.00	0 <sup>b</sup>	2	1.90	3.32	N/A
KAS28	Phalanx	Ovis/Capra	3.51 ± 0.06	0.25 ± 0.02	0.08 ± 0.01	0.48 ± 0.04	Absent	0.00	0 <sup>b</sup>	2	13.23	10.38	3.25
KAS29	Long bone	Ovis/Capra	3.91 ± 0.05	0.15 ± 0.01	0.06 ± 0.01	0.28 ± 0.01	Absent	0.00	0 <sup>b</sup>	2	10.23	8.88	3.26
Modern human 1	Femur	Human	3.35 ± 0.06	0.24 ± 0.02	0.18 ± 0.01	0.48 ± 0.02	N/A	N/A	N/A	N/A	N/A	N/A	N/A
Modern human 2	Femur	Human	3.36 ± 0.01	0.24 ± 0.00	0.18 ± 0.00	0.48 ± 0.01	N/A	N/A	N/A	N/A	N/A	N/A	N/A
Modern bovine	Femur	Cattle	3.22 ± 0.01	0.25 ± 0.01	0.22 ± 0.01	0.47 ± 0.02	N/A	N/A	N/A	N/A	N/A	N/A	N/A

$C/N \text{ collagen} = (\% C / \% N) \times (\text{atomic weight C} / \text{atomic weight N})$ ; R, right; L, left; P, proximal diaphysis; D, distal diaphysis; N/A, not assessed

<sup>a</sup> Collagen content estimates calculated using the equation collagen wt.% = 113.13 Am/P + 1.69 presented in Lebon et al. (2016)

<sup>b</sup> Samples with transverse thin sections

<sup>c</sup> Samples with longitudinal thin sections

was changed every 2 days. When demineralization was completed, the supernatant was drained off and samples were rinsed  $\times 3$  with distilled water. Gelatinization was carried out by adding 8 ml at pH 3 HCl, and samples were placed in hot blocks at 80 °C for 48 h. The supernatant which contains the collagen was filtered using Ezee™ filters and was freeze dried for 2 days in pre-weighed plastic tubes. Collagen yields (wt.%), which are commonly used to distinguish well-preserved from poorly preserved collagen were estimated using the formula: bone mass (mg)/collagen mass (mg)  $\times 100$ , where bone mass is the weight of bone chunks after cleaning the exterior surfaces, and collagen mass is the extracted material that remains following demineralization, gelatinization, and filtering.

The extracted collagen was analyzed in duplicate using a Sercon 20-22 mass spectrometer at the University of York (BioArCh) and following standard procedures. Thirty-six tin capsules containing 0.9–1.1 mg of collagen were dropped into an oxygen-rich combustion tube held at 1000 °C, while fifteen tin capsules of Bradford fish gel standard, three tin capsules of IA CANE (cane sugar), three tin capsules of IAEA 600 (caffeine), three tin capsules of IAEA N2 (ammonium sulfate), and three tin capsules of modern bovine collagen, all containing 0.9–1.1 mg of material, were used as standards. The tin capsules were ignited and burnt exothermally at 1800 °C causing the sample to oxidize.

The samples were carried through a layer of chromium oxide, and copper oxide which ensure complete oxidation, followed by a layer of silver wool to remove unwanted sulfur and halides. The sample gases then passed into a second furnace containing copper held at 600 °C where excess oxygen was removed and nitrogen oxides were reduced to elemental nitrogen. Any water was removed using a magnesium perchlorate trap. The samples then passed into a gas chromatography (GC) column held at 70 °C, which separates CO<sub>2</sub> and N<sub>2</sub> from each other. The resultant gases were then introduced into the mass spectrometer where the samples were ionized, and the various masses were separated in a magnetic field, focused into Faraday collector arrays and analyzed.

## Results and discussion

### Histological preservation

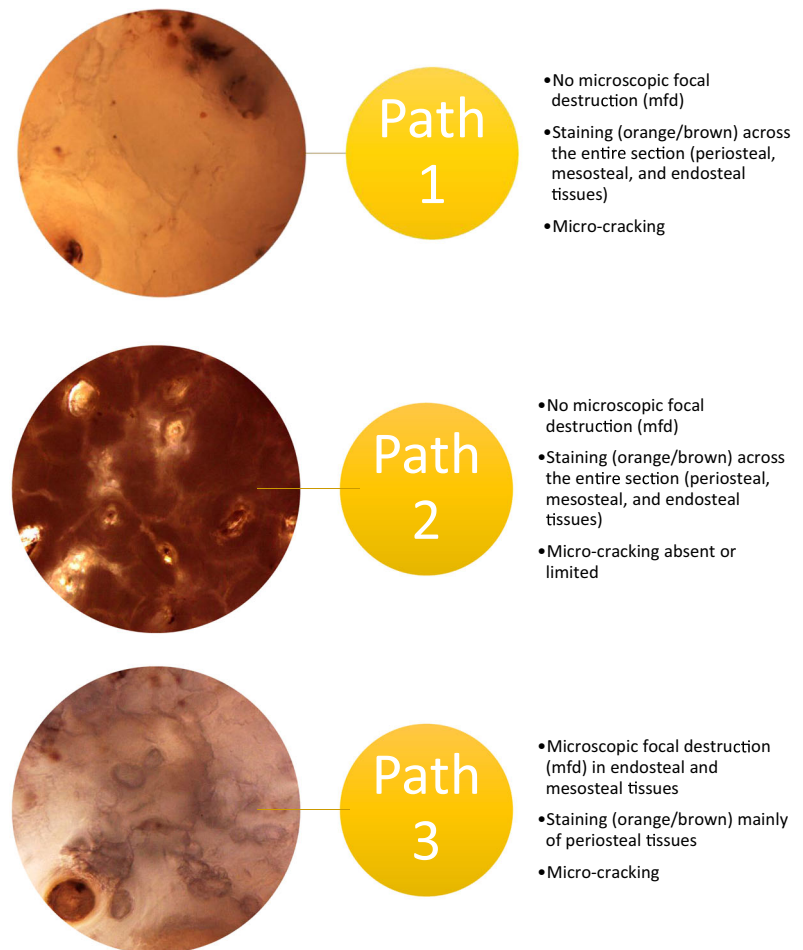
Histological preservation is very poor in Kastrouli (Table 1) with three distinct pathways identified based on the presence/absence of microscopic focal destruction (MFD), microcracking, and orange/brown staining (Fig. 2). All human femora and animal bones appear microstructurally amorphous with histology often displaying disintegration, although some limited morphological features may still be recognizable. Generalized destruction (Fig. 3a) is accompanied by a loss of birefringence in the amorphous areas under cross polarized

light, linked to a loss of collagen (Piepenbrink 1986; Garland 1989; Collins et al. 2002; Caruso et al. 2018). The two human petrous bones also have many amorphous, disintegrated areas of bone (Fig. 3b) accompanied by a loss of collagen birefringence, although the latter is still retained in many areas across the petrous thin sections. The endosteal tissue that surrounds the cochlea and semicircular canal areas is considered more mineralized (Doden and Halves 1984; Katić et al. 1991; Frisch et al. 2000; Jeffery and Spoor 2004), however, it is unexpectedly more degraded than the periosteal tissue.

Microscopic focal destruction (MFD) is present in nine human femora, while the two human petrous bones and all animal bones show no signs of bacterial attack (Table 1). Possible microbial activity in the two human petrous bones appears as merged osteocyte lacunae; however, these are very sparse (Fig. 3b). MFD in human femora appear as linear longitudinal (oval-shaped) and budded tunnels separated by hypermineralized tissue (or cuffing) (Fig. 4a). Cuffing displays a dark coloration (brown/black) in plane polarized light (Fig. 4a) and it appears denser than the unaffected areas (Hackett 1981; Piepenbrink 1989; Bell 1990). It is believed that it forms by mineral redeposition and waste products when microbes remove the inorganic matrix to attack collagen (Hackett 1981; Garland 1989; Jackes et al. 2001; Hedges 2002; Fernandez-Jalvo et al. 2010), which explains why it has higher concentrations of Ca and P compared with the unaffected bone (Pesquero et al. 2015). This hypermineralized tissue is a few micrometers in size, mostly surrounding the smaller non-Wedl MFD (Fig. 4a), and it inhibits further expansion of the MFD (Hackett 1981; Piepenbrink 1986). The “mosaic pattern” observed in Fig. 4b is also considered to be the final stage of bacterial attack, removing almost all microstructural features (Hackett 1981; Piepenbrink 1986; Turner-Walker and Jans 2008).

Groundwater fluctuation in Kastrouli (Fig. 5) due to hot and dry summers (desiccation, which causes the bone to shrink) followed by cold and humid winters (water uptake that swells bone collagen) has played a key role in altering bone and has resulted in the poor histological preservation (Hackett 1981; Hedges and Millard 1995; Nielsen-Marsh and Hedges 2000a; Turner-Walker 2008; Turner-Walker and Jans 2008; Pfretzschner and Tütken 2011). Desiccation is evidenced by microcracks (Pfretzschner and Tütken 2011) observed centrally (Fig. 4a; spread from the Haversian canal outwards), peripherally (Fig. 4a; spread from the cement line inwards), circumferentially, and interstitially (Fig. 4c; run across circumferential and interstitial lamellae) in several bones. Additionally, the wet and dry (oxygen-rich environment) cycles in Kastrouli also favor the survival and activity of microorganisms in bone (Hackett 1981; Reiche et al. 2003; Turner-Walker and Jans 2008), while microcracking would further accelerate protein degradation and mineral transformation by increasing the flow of groundwater through the bone.

**Fig. 2** The three different diagenetic pathways histologically identified in Kastrouli bones (see also Table 1)



## Bioapatite preservation

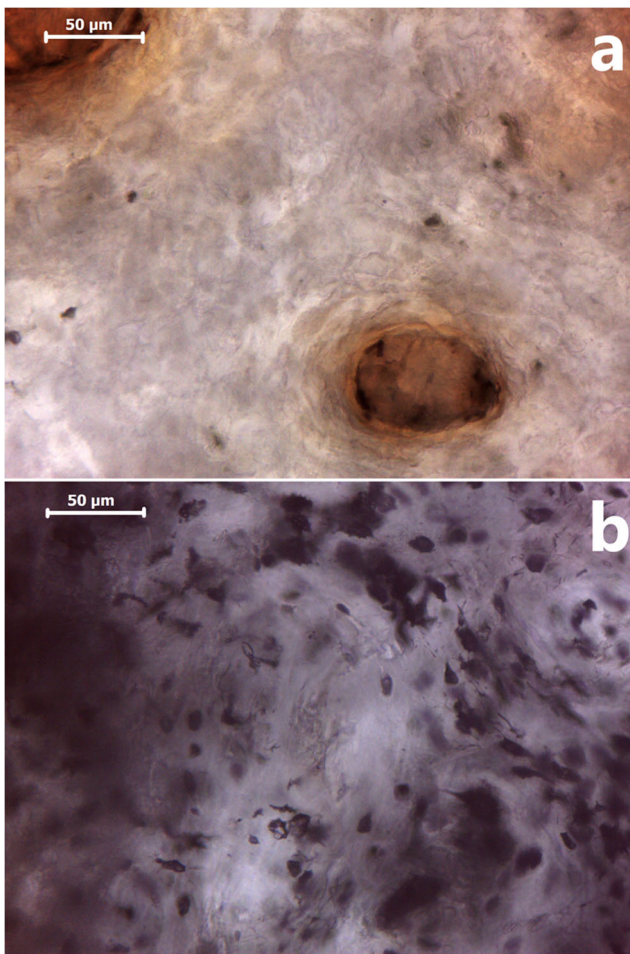
Dissolution/recrystallization of BAp crystals in Kastrouli is indicated by the histological appearance of many samples (e.g., microcracking, loss of birefringence). A combination of flow and recharge hydrological environments (Hedges and Millard 1995; Nielsen-Marsh et al. 2000) has clearly affected bioapatite preservation at this site. The seasonal or sporadic (wet and dry cycles; Fig. 5) flow of undersaturated (with respect to BAp) rainwater (Grupe 1995; Hedges and Millard 1995; Nielsen-Marsh et al. 2000) through the bones situated near the ground surface (depth c. 1 m) has led to the recrystallization of bioapatite crystals.

The IRSF values range from 3.37 to 5.47 (mean =  $4.38 \pm 0.69$ ) in human bones and from 3.51 to 4.10 (mean =  $3.69 \pm 0.23$ ) in animal bones. These crystallinity values are higher than the modern human bone references' mean IRSF value (i.e.,  $3.36 \pm 0.01$ ; Fig. 6a) and indicate an expansion of the crystal dimensions. This increase may be due to Ostwald ripening (larger crystals absorb the smaller ones), loss of the smaller crystals through dissolution, or both (Weiner and

Bar-Yosef 1990; Stiner et al. 1995; Wright and Schwarcz 1996; Nielsen-Marsh and Hedges 2000b; Nielsen-Marsh et al. 2000; Reiche et al. 2002; Trueman 2013). To assess whether the distribution (mean ranks) of crystallinity (IRSF) values between the human ( $n = 17$ ; including the two petrous bones) and animal ( $n = 7$ ) bones is different, a Mann-Whitney U test was used as the IRSF values were not normally distributed in the latter group (Shapiro-Wilk:  $p = 0.031$ ). The statistical analysis indicated that the human bones (mean rank = 14.82) tend to have higher crystallinity values than the animal bones (mean rank 6.86) ( $U = 20.000$ ,  $p = 0.011$ ).

Regarding the carbonate content, C/P ranges from 0.23 to 0.08 (mean =  $0.15 \pm 0.05$ ) in human bones, and from 0.25 to 0.15 (mean =  $0.20 \pm 0.05$ ) in animal bones. Similarly, as normality was not met in the animal bones (Shapiro-Wilk:  $p = 0.042$ ), a Mann-Whitney U test indicated that the animal bones (mean rank = 17.86) have higher C/P values than the human bones (mean rank = 10.29) in Kastrouli ( $U = 22.000$ ,  $p = 0.016$ ). A loss of  $\text{CO}_3^{2-}$  content during dissolution/recrystallization is thus observed in our samples compared with modern samples (Fig. 6a). The human bones display an average

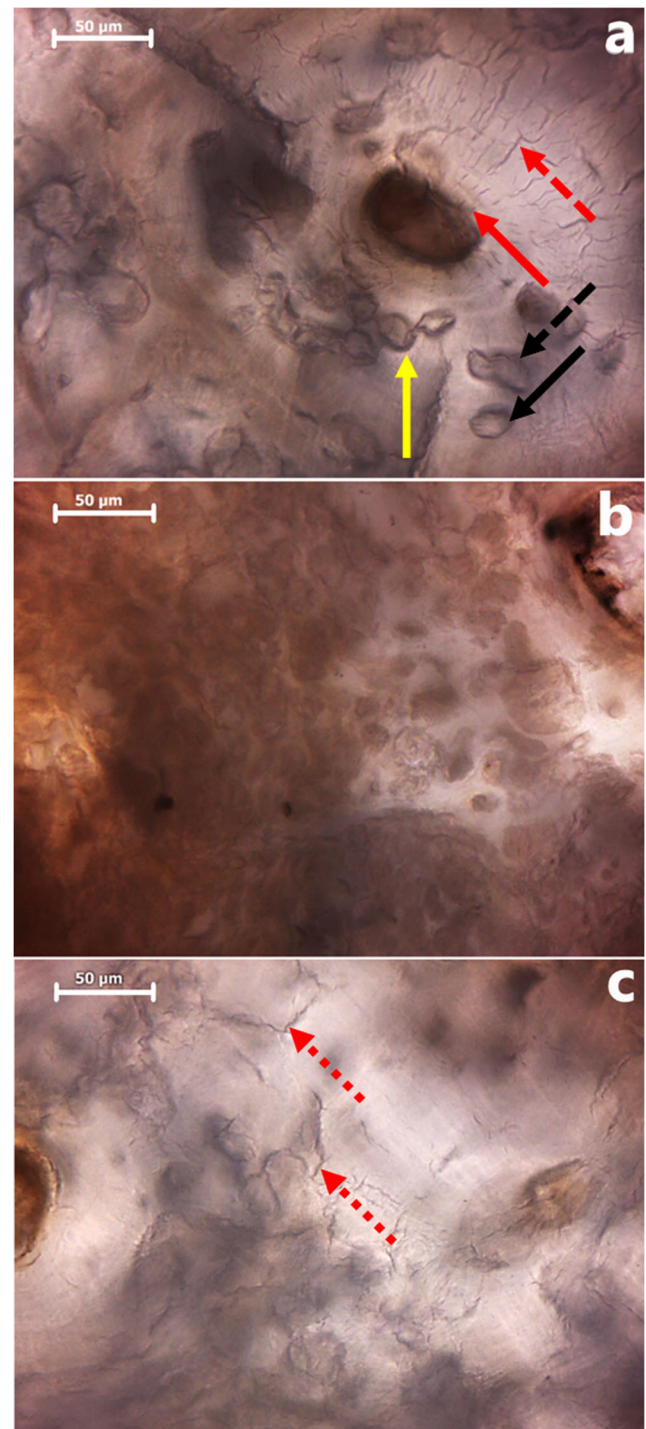




**Fig. 3** **a** KAS2 transverse PPL  $\times 400$ —human femur: no histological features can be recognized, accompanied by a complete loss of birefringence (hence no image). **b** KAS16 longitudinal PPL  $\times 400$ —human petrous bone: osteocyte lacunae still preserved. Note the few merged lacunae which can be an indication of limited microbial activity.

loss of about 40% of the initial carbonate and the animal bones of about 20% of their initial  $\text{CO}_3^{2-}$ , although the average crystal size and atomic disorder vary between animal species and hard tissues (Asscher et al. 2011).

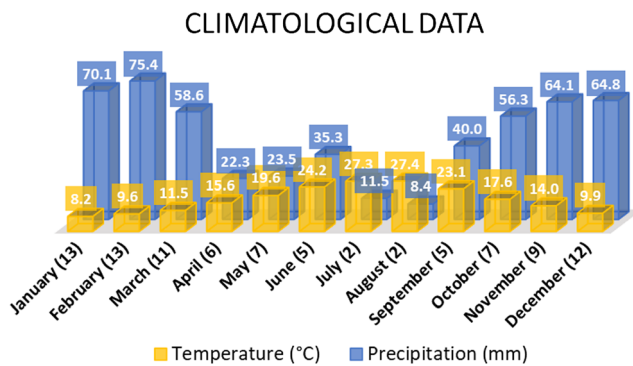
The IRSF and the C/P ratios display a very strong inverse correlation for the human bones ( $R^2 = 0.87$ ) and a strong inverse correlation for the animal bones ( $R^2 = 0.61$ ). This indicates that while recrystallization in bones results in a loss of carbonate from the bioapatite crystals, this loss of  $\text{CO}_3^{2-}$  can vary within the same site and between different species (Fig. 6a, b). There are also statistically significant differences in crystallinity ( $F(2) = 22.260$ ,  $p = 0.000$ ) and C/P ( $F(2) = 6.989$ ,  $p = 0.006$ ) between the three different diagenetic pathways described at the site. The use of the one-way ANOVA test indicated that the diagenetic pathway 1 ( $n = 4$ ) displays the poorest inorganic preservation with very high crystallinity values (IRSF =  $5.4 \pm 0.06$ ) and very low carbonate content (C/P =  $0.09 \pm 0.01$ ) which is statistically significant different compared with the other two diagenetic pathways (IRSF:



**Fig. 4** **a** KAS9 transverse PPL  $\times 400$ —human femur: MFD in the form of linear-longitudinal (black arrow) and budded (dashed black arrow) tunnels surrounded by hypermineralized tissue (yellow arrow). Note the central (red arrow) and peripheral (dashed red arrows) microcracks. **b** KAS13 transverse PPL  $\times 400$ —human femur: the characteristic “mosaic pattern” attributed to extensive bacterial activity. **c** KAS1 transverse PPL  $\times 400$ —human femur: microcracking in degraded interstitial lamellae (dotted red arrows).

diagenetic pathway 1 vs. pathway 2,  $p = 0.000$ ; IRSF: diagenetic pathway 1 vs. pathway 3,  $p = 0.000$ ; C/P: diagenetic





**Fig. 5** Mean monthly temperatures (°C) and precipitation (mm) from January 2010 to January 2019 measured at the nearby Antikira weather station (38° 24' N 22° 36'; elevation, 336 m). The measurements were made on a continuous basis every 10 min from 01.01.2010 to 31.01.2019. The average days of precipitation for each month over this 9-year period is provided in parenthesis. The climatological data are available through the National Observatory of Athens, Greece (see Moustris and Petrou 2019)

pathway 1 vs. pathway 2,  $p = 0.004$ ; C/P: diagenetic pathway 1 vs. pathway 3,  $p = 0.023$ ). The diagenetic pathway 3 ( $n = 9$ ) shows intermediate values with lower crystallinity ( $\text{IRSF} = 3.97 \pm 0.44$ ) and slightly higher  $\text{CO}_3^{2-}$  values ( $\text{C/P} = 0.12 \pm 0.04$ ), and compared with the diagenetic pathway 2 ( $n = 8$ ) that demonstrates the best BAp preservation with  $\text{IRSF} = 3.89 \pm 0.43$  and  $\text{C/P} = 0.19 \pm 0.05$ , there is no statistically significant difference ( $\text{IRSF } p = 0.904$ ;  $\text{C/P } p = 0.569$ ).

Carbonate ions (4–6 wt.%) can be exchanged with  $\text{OH}^-$  (type A) or  $\text{PO}_4^{3-}$  (type B) ions in the bioapatite crystal lattice (LeGeros 1965; Wopenka and Pasteris 2005). Type A substitutions require 900–1000 °C, hence no water, while type B substitutions are the dominant substitutions in bone as they occur at 25–100 °C (LeGeros 1965). The very strong linear relationship ( $R^2 = 0.85$ ; Fig. 6c, d) between the c. 1410  $\text{cm}^{-1}$  peak and the c. 872  $\text{cm}^{-1}$  peak that is also assigned to type B carbonate (Elliott 1964; LeGeros et al. 1969; Rey et al. 1989) shows that C/P (1410  $\text{cm}^{-1}$ /1035  $\text{cm}^{-1}$ ) predominantly reflects the type B  $\text{CO}_3^{2-}$  environment (Sponheimer and Lee-Thorp 1999). A substitution of  $\text{CO}_3^{2-}$  by  $\text{PO}_4^{3-}$  during recrystallization increases the unit cell dimensions of BAp crystals, as  $\text{PO}_4^{3-}$  O–O distances are longer than these in  $\text{CO}_3^{2-}$  (LeGeros et al. 1969), while it also results to more ordered crystal lattices (LeGeros 1965; LeGeros et al. 1967; Wopenka and Pasteris 2005; Rey et al. 2007). When crystallinity (IRSF) is plotted against type B  $\text{CO}_3^{2-}$  (BPI); however, it appears that the exchange of ions at the type B  $\text{CO}_3^{2-}$  site has less impact on BAp crystals of animal bones than in humans (Fig. 6e, f), which implies differences in the diagenetic pathways followed by human and animal bones in Kastrouli.

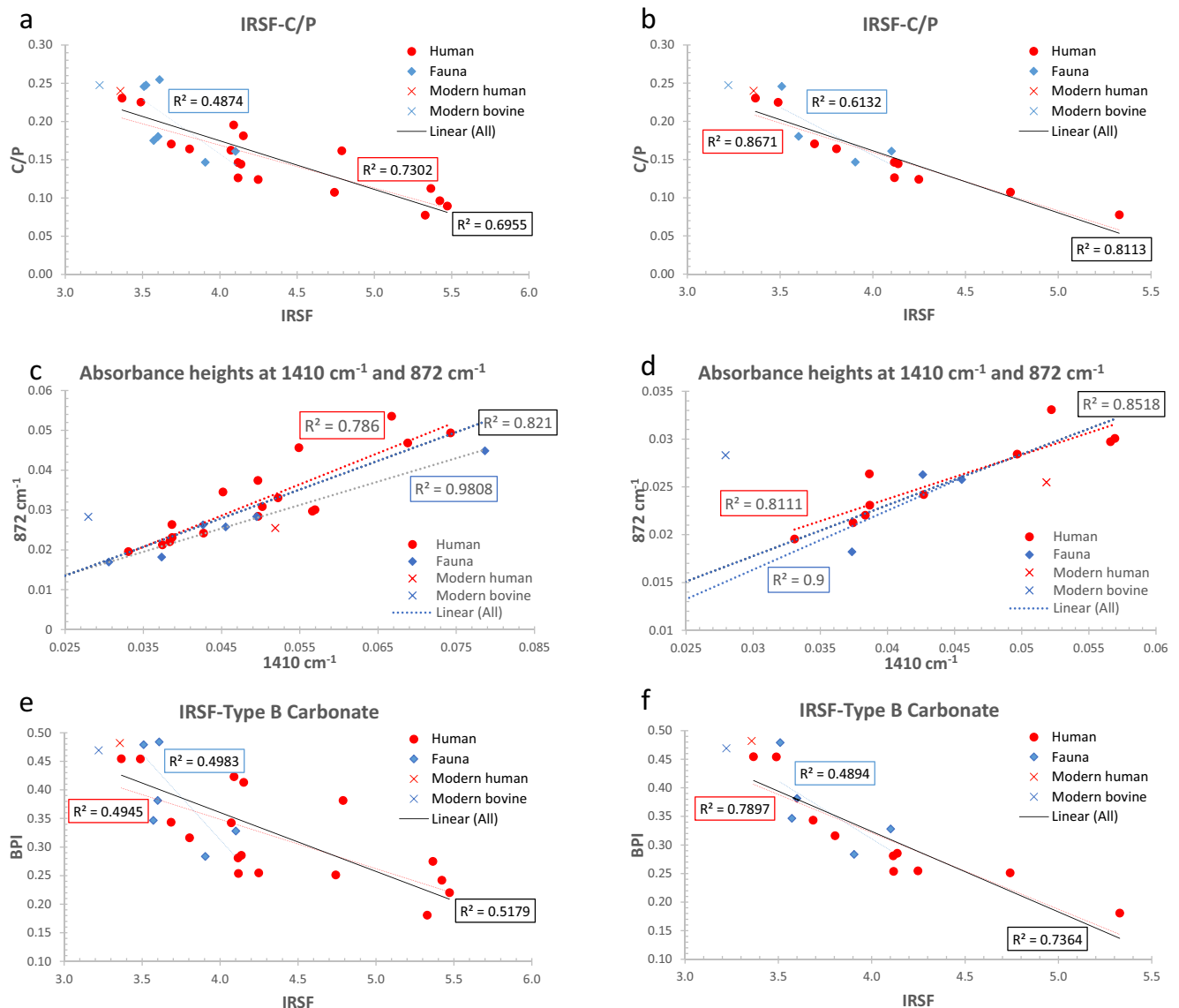
Calcite ( $\text{CaCO}_3$ ) is identified in ten samples (Table 1) primarily by the presence of a peak at 712  $\text{cm}^{-1}$  ( $\nu_4$  carbon-oxygen in-plane bending) (Hunt et al. 1950; Baxter et al. 1966), while changes in the absorbance heights of the 872  $\text{cm}^{-1}$   $\nu_2$  carbon-

oxygen out-of-plane bending and the 1410  $\text{cm}^{-1}$   $\nu_3$  carbon-oxygen asymmetric stretching (Elliott 1964; Baxter et al. 1966; LeGeros et al. 1969; White 1974) have also provided useful information. The strong linear relationship ( $R^2 = 0.71$ ) between the  $\nu_4$  (712  $\text{cm}^{-1}$ ) and the  $\nu_2$  (872  $\text{cm}^{-1}$ ) vibration modes in our samples compared with the weak correlation ( $R^2 = 0.2$ ) between the  $\nu_3$  (1410  $\text{cm}^{-1}$ ) and the  $\nu_4$  (712  $\text{cm}^{-1}$ ) suggests that the former modes are more sensitive indicators of calcite in archaeological bone. The 712  $\text{cm}^{-1}$  is considered characteristic of the changes in the Ca–O distance during vibration which is three times larger for the  $\nu_4$  mode compared with the  $\nu_2$  mode (Gueta et al. 2007).

The carbonate moieties are coplanar and the  $\text{O}_1\text{--O}_2$  distance affects the in-plane bending vibration ( $\nu_4$  mode) more than the out-of-plane bending vibration ( $\nu_2$  mode) (Gueta et al. 2007). This is important for the distinction between a rather amorphous bone calcium carbonate (lower order with greater Ca–O and  $\text{O}_1\text{--O}_2$  distances) and exogenous calcite (higher order with smaller distances) (Gueta et al. 2007). The mean  $\text{IRSF} = 4.41 \pm 0.79$  and  $\text{C/P} = 0.17 \pm 0.06$  for samples displaying calcite uptake compared with  $\text{IRSF} = 4.01 \pm 0.53$  and  $\text{C/P} = 0.16 \pm 0.05$  in samples without calcite demonstrates how the calcite uptake increases BAp crystal order (increased IRSF).

The  $\nu_2$  carbonate band at c. 850–900  $\text{cm}^{-1}$  which is considered free of organic constituents (Termine et al. 1973) and generally free of  $\text{HPO}_4^{2-}$  artifacts (Rey et al. 1989) also offers useful information through 2<sup>nd</sup> derivative analysis (Fig. 7). The two main carbonate bands in modern bone at c. 879 and c. 871  $\text{cm}^{-1}$ , which appear slightly shifted in archaeological bone, are frequently assigned to type A (stuffed, i.e., located in the crystal channel and oriented with two oxygen atoms close to the  $c$ -axis) and type B (positioned close to the sloping faces of the phosphate tetrahedron) carbonates, respectively (LeGeros 1965; LeGeros et al. 1967; Rey et al. 1989; Fleet and Liu 2004, 2005; Fleet et al. 2004; Fleet 2009). A gradual increase in the 871  $\text{cm}^{-1}$  component is observed that is accompanied by a loss of the 879  $\text{cm}^{-1}$  component with increasing calcite content (712  $\text{cm}^{-1}$  absorbance height) in bones from Kastrouli (Fig. 7) that is not reflected in C/P values likely due to small variations of the lattice dimensions of the substituents (Rey et al. 1989).

Therefore, the 2<sup>nd</sup> derivative analysis of the  $\nu_2$   $\text{CO}_3^{2-}$  mode potentially indicates that an uptake of calcite (or its formation from dissolved carbonate ions and free calcium ions present in water (Fernández-Jalvo et al. 2016)) may occur at the sloping faces of BAp crystals, replacing type B  $\text{CO}_3^{2-}$  during the interaction of bone with groundwater in the burial environment (Wright and Schwarcz 1996; Maurer et al. 2014). This uptake of calcite from the burial environment may be either accompanied by a gradual loss of the type A carbonate (disappearance of the 879  $\text{cm}^{-1}$  component, i.e., complete



**Fig. 6** **a** The relationship between crystallinity (IRSF) and carbonate content (C/P) in BAp crystals. **b** Same as (a), excluding samples containing calcite. **c** Correlation between 1410 and 872  $\text{cm}^{-1}$  showing that type B carbonate is the main  $\text{CO}_3^{2-}$  type reflected in C/P values. **d** Same as (c),

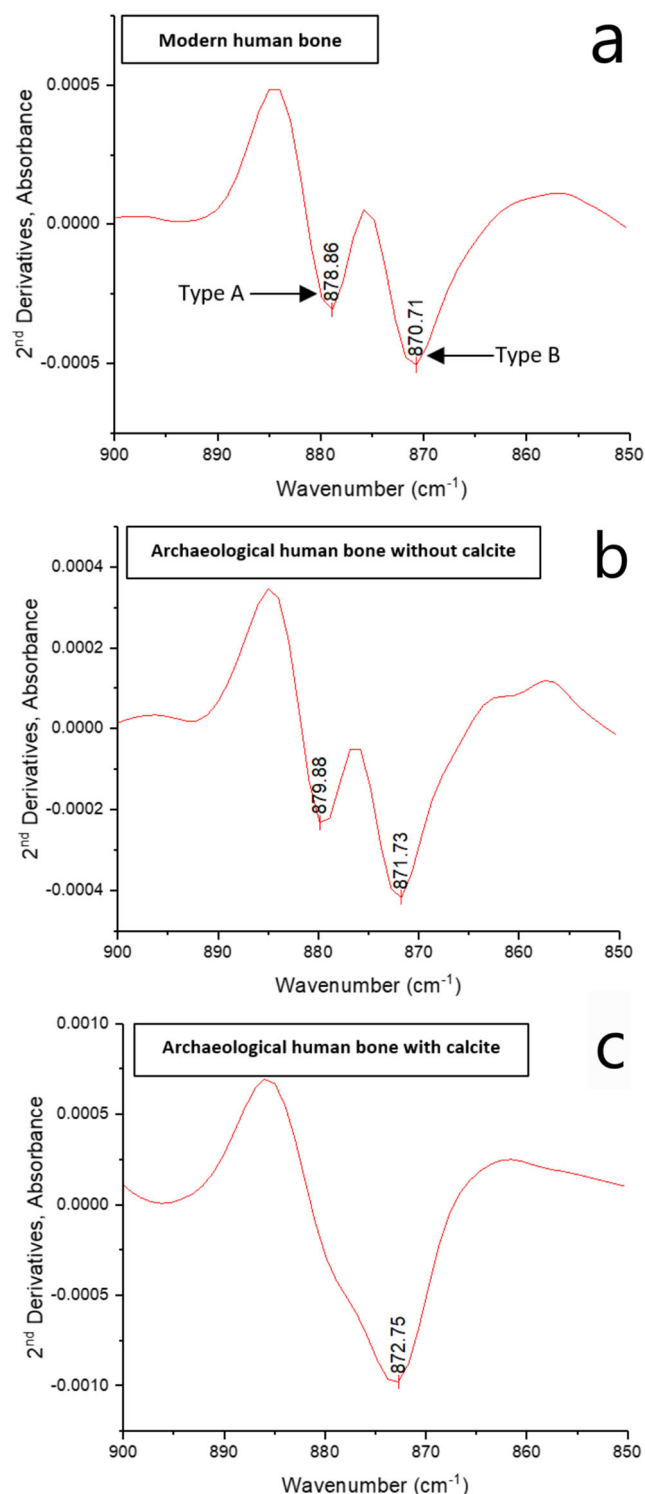
excluding samples containing calcite. **e** The relationship between crystallinity (IRSF) and type B  $\text{CO}_3^{2-}$ . **f** Same as (e), excluding samples containing calcite

transformation of BAp) during severe dissolution of the crystal, and/or the exogenous carbonate/calcite vibrations mask the c. 879  $\text{cm}^{-1}$  component (i.e., partial transformation of BAp). As the  $\text{CO}_3^{2-}$  for  $\text{OH}^-$  substitution is achieved only with the exclusion of water, it is difficult for type A substitution to occur in bioapatite (LeGeros et al. 1969).

Finally, the presence of the c. 866  $\text{cm}^{-1}$  component which has been observed in modern bone and it has been linked to non-apatitic (labile) carbonate environment in amorphous calcium carbonate (Elliott 1964; Rey et al. 1989) is not observed in the 2<sup>nd</sup> derivative spectra of the Kastrouli bones (Fig. 7). Its absence from archaeological bone has been reported in previous studies (Kontopoulos et al. 2018), although contrary to this data, Stathopoulou et al. (2008) observed the 866  $\text{cm}^{-1}$

component in fossilized bones and it increases with increasing crystallinity.

The spectra in the  $\nu_3$  carbon-oxygen asymmetric stretching mode (c. 1400–1600  $\text{cm}^{-1}$ ) are very complex (Fig. 8). The 2<sup>nd</sup> derivative analysis of this domain shows that almost all the components decrease to different extents in archaeological bone compared with modern bone, except for the 1451  $\text{cm}^{-1}$ , the 1501  $\text{cm}^{-1}$ , and the 1517  $\text{cm}^{-1}$  peaks that remain relatively unchanged (Fig. 8a, b). However, the archaeological bone with calcite uptake shows different characteristics (Fig. 8c). Specifically, there is an increase in the slightly shifted 1411  $\text{cm}^{-1}$  component, and a small increase in the 1468  $\text{cm}^{-1}$  and 1551  $\text{cm}^{-1}$  peaks (Fig. 8c) compared with the archaeological bone without calcite (Fig. 8b). These changes are accompanied



**Fig. 7** Second derivative spectra of the  $\nu_2$  carbonate band at c. 850–900  $\text{cm}^{-1}$  of modern human bone (**a**) and two archaeological human bones with C/P = 0.16 but different calcite amounts (**b** KAS13; **c** KAS3). Note the effect on the 879  $\text{cm}^{-1}$  component when there is an uptake of calcite (**b** vs. **c**)

by a decrease in the 1535  $\text{cm}^{-1}$  and 1568  $\text{cm}^{-1}$  components, whereas the remaining peaks appear unchanged (Fig. 8c).

A decrease in the 1468  $\text{cm}^{-1}$  and 1536  $\text{cm}^{-1}$  peaks can be possibly related to loss of type A  $\text{CO}_3^{2-}$  (Rey et al. 1989; Madupalli et al. 2017), while a decrease in the 1411  $\text{cm}^{-1}$  peak in the archaeological bone without calcite uptake can be linked to a loss of type B structural carbonate (Rey et al. 1989; Fleet and Liu 2004). This is also reflected in the decreased, compared with modern bone, C/P ratio of KAS13. On the other hand, an increase in the 1411  $\text{cm}^{-1}$  peak in the specimen with calcite uptake possibly indicates the position that calcite predominantly occupies in BAP crystals (i.e., type B). Lastly, a decrease of the 1536  $\text{cm}^{-1}$  and 1552  $\text{cm}^{-1}$  components (Fig. 8) may also be attributed to a loss of organic content (amide II) (Paschalis et al. 2001; Chadeaux et al. 2009).

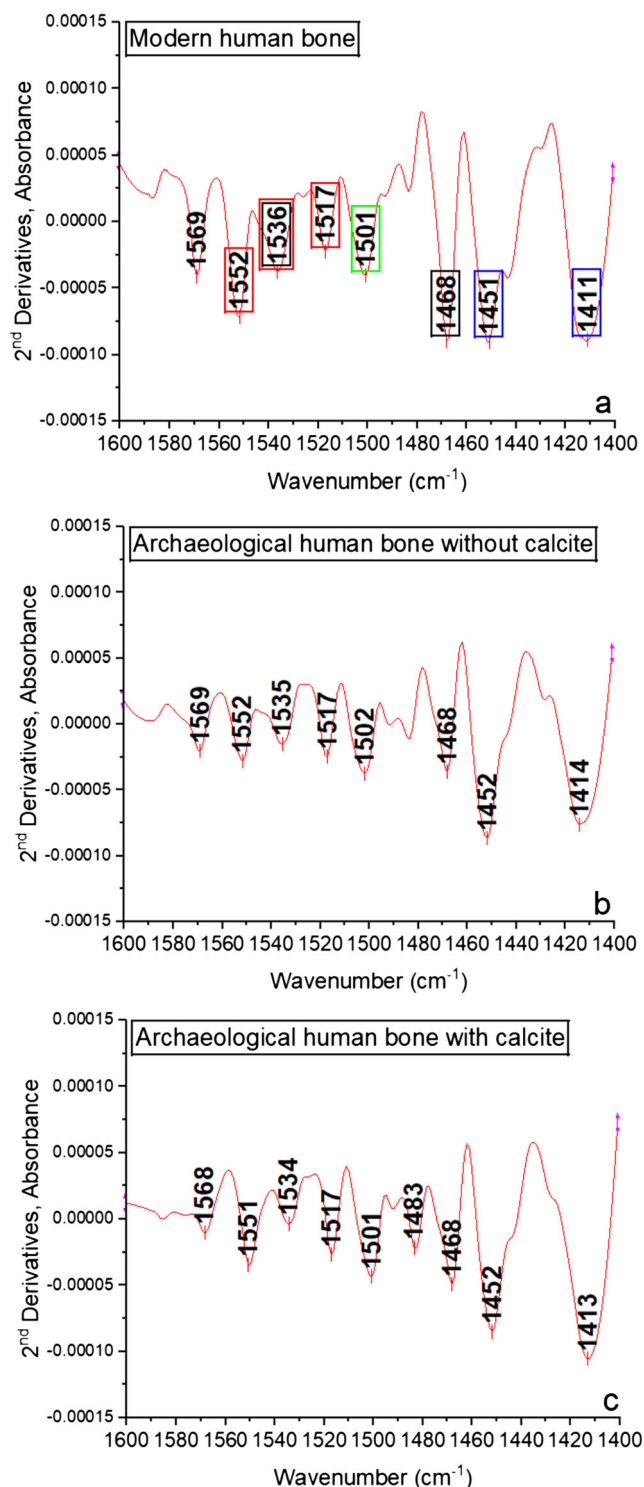
Combined, it seems that there is a loss of some A site components both in the  $\nu_3$  and the  $\nu_2$  modes and a co-precipitation of exogenous carbonate and phosphate in B sites. An A site carbonation in the apatitic *c*-axis channel would require much higher energy than B site carbonation of phosphate sites (Madupalli et al. 2017); thus a loss of type A carbonate during partial BAP crystal dissolution, followed by recrystallization and incorporation of exogenous  $\text{CO}_3^{2-}$ , is more probable. Additionally, exogenous carbonate may be positioned differently and these changes observed in the 2<sup>nd</sup> derivative components could be caused by the changes in carbonate orientation (Madupalli et al. 2017). It is also likely that the hypothesis of two carbonate environments, each of which has its own characteristic absorption spectrum, might be an oversimplification, while the allocation of specific derivative peaks to each  $\text{CO}_3^{2-}$  type requires further exploration (Elliott 1964; Elliott et al. 1985).

It is difficult to make any safe assumptions on the location of exogenous  $\text{CO}_3^{2-}$  in the BAP crystal lattice due to the extensive overlapping and a variation in peak positions for the carbonate ion (Fleet and Liu 2004). The many bands and shoulders displayed in these regions are still not safely assigned to a specific  $\text{CO}_3^{2-}$  site (Elliott 1964; LeGeros et al. 1969; Rey et al. 1989), and apart from carbonate, some domains also include absorption from other bands (e.g., CH, CN,  $\text{COO}^-$ , NH) that overlap with  $\text{CO}_3^{2-}$  (Elliott 1964; Termine et al. 1973) and hinder further interpretation.

### Collagen preservation

Collagen preservation displays within-site variations, ranging from 0.86 to 12.07 wt.% (mean = 6.73) in human specimens, and between 1.90 and 13.23 wt.% (mean = 8.35) in animal bones (Table 1). A *t* test indicated no statistically significant differences between the two groups in collagen wt.% (*t* (22) = 48.000, *p* = 0.352), although the number of samples was small (human bones *n* = 17; animal bones *n* = 7). Further, a one-way ANOVA test was also performed to determine whether the three different diagenetic pathways display statistically significant differences in collagen yields. The collagen yields





**Fig. 8** The complex 2nd derivative spectra of the  $\nu_3$  carbonate mode (c. 1400–1600  $\text{cm}^{-1}$ ) of modern human bone (a) and two archaeological human bones with C/P=0.16 but different calcite amounts (b KAS13; c KAS3) Black boxes highlight the possible type A carbonate components; blue boxes highlight the possible type B carbonate components; green box highlights a possible non-apatitic (labile) carbonate component; red boxes highlight the possible organic (amide II) components (Termine et al. 1973; Rey et al. 1989; Fleet and Liu 2004; Brangule and Gross 2015; Madupalli et al. 2017)

(wt.%) are statistically significant different between those three groups ( $F(2) = 6.471$ ,  $p = 0.008$ ) as the diagenetic pathway 1 displays very poor collagen preservation (collagen wt.% =  $1.8 \pm 1.06$ ) compared with the other two diagenetic pathways (diagenetic pathway 1 vs. pathway 2:  $p = 0.019$ ; diagenetic pathway 1 vs. pathway 3:  $p = 0.007$ ). The diagenetic pathway 2 mean collagen yield is  $7.56 \pm 3.69$ , and the diagenetic pathway 3 displays slightly higher mean collagen yield ( $8.32 \pm 3.08$ ) which are not statistically significantly different ( $p = 0.873$ ).

Collagen C/N ratios were used for quality assessment with values ranging from 3.19 to 3.99 (Table 1). Values similar to modern bone (i.e., 2.9 to 3.6) are considered representative of good-quality collagen, while higher C/N ratios are related to diagenesis (DeNiro 1985; DeNiro and Weiner 1988; Ambrose 1990; Tuross 2002). Only three human specimens with diagenetic pathway 1 characteristics (KAS1, KAS7, KAS15) exhibit C/N > 3.6 (Table 1). These samples also show calcite uptake, while KAS7 and KAS15 have collagen yields below the 1 wt.% that is currently considered the threshold for isotopic and/or radiocarbon dating studies (van Klinken 1999; Dobberstein et al. 2009; Brock et al. 2010, 2012). Thus, collagen retained within these bones may not purely reflect original biochemical signals.

Apart from the uptake of exogenous carbon, post-mortem alterations in the collagen carbon and nitrogen contents are affected by microbial attack and hydrolysis (Ambrose 1990; Hedges et al. 1995; Balzer et al. 1997; Tuross 2002; Turner-Walker 2008; Harbeck and Grupe 2009). Hydrophobic amino acids may have been hydrolyzed during wet periods in Kastrouli, whereas a possible microbial attack to the amino acids with a higher number of carbons may have also occurred in samples displaying MFD, altering the C/N ratio (Masters 1987; Grupe 1995; Balzer et al. 1997; Turban-Just and Schramm 1998; Tuross 2002; Harbeck and Grupe 2009).

While bone may preserve its microstructure without preserving its collagen content due to hydrolysis (Hedges et al. 1995; Collins et al. 2002), in this secondary Mycenaean burial poor histological preservation is often accompanied by good collagen preservation (Table 1). This observation shows that many bones can still retain appreciable quantities of protein even after extensive histological alterations (Hedges et al. 1995) and highlights the limitations of GHI's use as a collagen indicator.

The interaction between the mineral and organic fractions of bone is generally considered strong during diagenesis (Person et al. 1995, 1996; Nielsen-Marsh et al. 2000). This view is based on the fact that the orientation and size of BAP crystals *in vivo* are controlled by the fibril structure and organization as they are situated between (inter-fibrillar spaces) or on the surfaces (intra-fibrillar spaces) of collagen fibrils (Weiner and Traub 1986; Weiner and Price 1986; Boskey 2003). However, in Kastrouli only a moderate correlation

between crystallinity (IRSF) and collagen content ( $R^2 = 0.44$ ) is observed (Fig. 9a), something that has also been reported in past studies (Lebon et al. 2010; Weiner and Bar-Yosef 1990; Hedges et al. 1995). Thus, our data suggest that bioapatite recrystallization is possible even in the presence of reasonable amounts of collagen in bone (Reiche et al. 2003), while within the same burial environment the volume of bone matrix that is filled with collagen *in vivo* can be replaced by BAp crystals of increased size (Trueman et al. 2008b; Susini et al. 1988; Pfretzschner 2004).

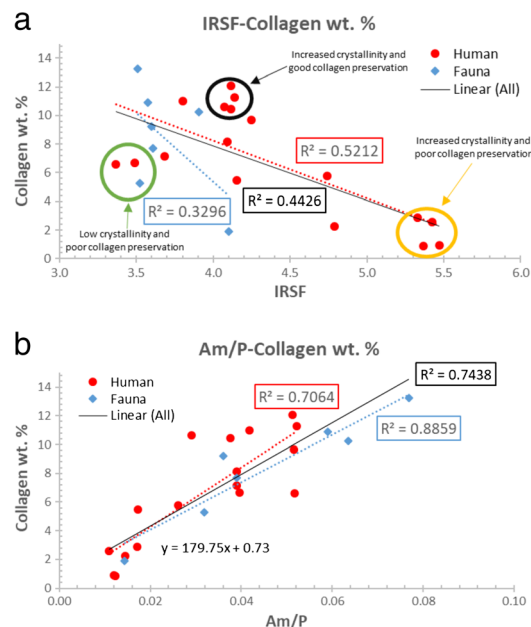
The Am/P ratio shows a strong correlation ( $R^2 = 0.74$ ) with collagen wt.% (Fig. 9b) which highlights the potential of Am/P as collagen predictor for rapid screening. The application of the Am/P ratio as a quantitative approach to estimate collagen yields using the Lebon et al. (2016) equation (i.e., collagen wt.% =  $113.13 \text{ Am/P} + 1.69$ ), however, displays a mean offset of  $-0.94 \pm 1.37\%$  in Kastrouli. The relative phosphate content can lead to poor agreement of collagen estimates with collagen yields in some specimens (e.g., KAS8, KAS9), while overtones related to O-H stretching vibrations at  $1640\text{--}1660 \text{ cm}^{-1}$  (structural water) can also lead to increased values (Trueman et al. 2008a; Lebon et al. 2016). Further, any differences in collagen and FTIR protocols can also have significant effects on the collagen content estimates (e.g., Sealy et al. 2014; Kontopoulos et al. 2018).

Additional qualitative evidence can be obtained through the 2<sup>nd</sup> derivative analysis of the amide I band that shows a gradual decrease of the  $1632 \text{ cm}^{-1}$ ,  $1640 \text{ cm}^{-1}$ , and  $1650 \text{ cm}^{-1}$  components assigned to the polyproline II helix (Lazarev et al.

1985) with decreasing collagen yields in archaeological bone (Fig. 10). Cleavage of collagen cross-linking as seen from a decrease of the  $1660 \text{ cm}^{-1}$  and  $1695 \text{ cm}^{-1}$  components (Fig. 10) (Paschalis et al. 2001) has led to a loss of the three-dimensional structure and breaking of the polypeptides into smaller peptides during hydrolysis (Collins et al. 1995, 2002; Shoulders and Raines 2009; Adzhubei et al. 2013). High average temperatures have also significantly affected the rate of collagen degradation in Kastrouli bones as higher temperatures accelerate collagen loss resulting in the thermal age at Kastrouli (Fig. 5) estimated to be approximately three times the real age (Collins et al. 2002; Kendall et al. 2018).

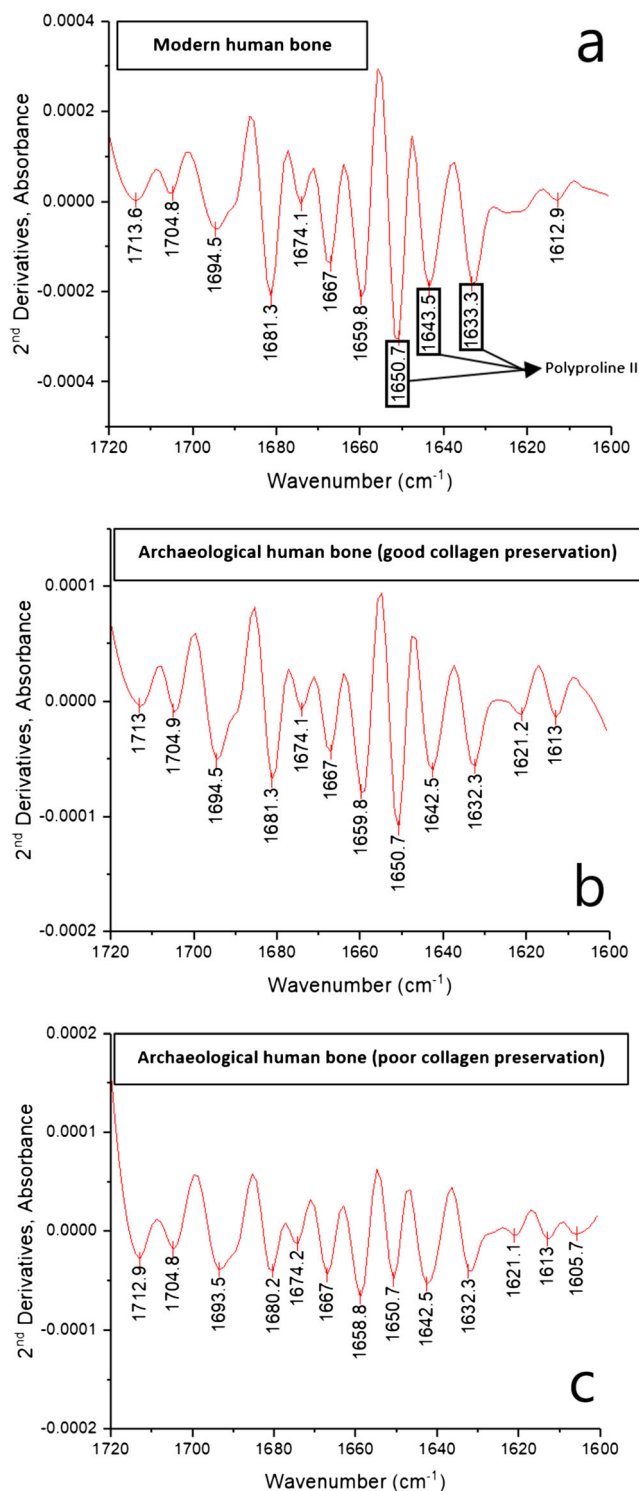
## Summary

Skeletal remains in this Mycenaean secondary burial have been seriously affected by diagenesis. Post-mortem modifications observed in microstructure, bioapatite, and collagen are characteristic of burial environments with groundwater fluctuation and high average temperatures. Within-site differences may be related to different microenvironment conditions (e.g., groundwater, contact with limestone bedrock). However, as all bones were found within 30 cm of sediment, these bones have possibly experienced different early taphonomic histories. The death history and the effects of various factors (e.g., season of death, clothing, burial location) on bone degradation are often overlooked in archaeology due to lack of relevant information. In



**Fig. 9** **a** The moderate relationship between IRSF-collagen wt.%. Note the group characterized by high IRSF and low collagen yields (yellow circle), a second group that displays low IRSF and low collagen yields (green circle) and a third group showing increased crystallinity and high

collagen yields (black circle), indicative of the different combination of diagenetic pathways followed by these specimens. **b** The reliability of Am/P for predicting collagen content in archaeological bone.



**Fig. 10** **a** Second derivative spectra of the amide I band (c. 1600–1700  $\text{cm}^{-1}$ ) showing the disappearance of amide I components (black boxes) that accompany loss of collagen in archaeological bone (**b** KAS8; **c** KAS7)

secondary burials, the skeletal remains of a body (either exposed on the ground surface, interred in a coffin or buried directly into the soil) are retrieved and relocated once

the soft tissue has decayed to some degree or excarnated. Therefore, future analyses may help understand the sequence of these alterations and shed light on past funerary practices such as disarticulation and primary and secondary treatments.

## Key points

### Histology

1. Three distinct diagenetic pathways were identified based on the presence/absence of microscopic focal destruction, microcracking and orange/brown staining of bone tissue.
2. Generalized destruction was observed in all human femora and animal bones.
3. The two human petrous bones show moderate histological preservation, and the endosteal tissue that surrounds the cochlea and semicircular canal areas is unexpectedly more degraded than the other tissue zones.

### Bioapatite

1. The seasonal and sporadic flow of rainwater through the bones which were situated near the ground surface (depth c. 1 m) likely led to the dissolution and recrystallization of bioapatite crystals (increased crystallinity, loss of carbonate, calcite uptake).
2. The two human petrous bones show poor bioapatite preservation with high crystallinity and loss of carbonate content.
3. 2<sup>nd</sup> derivative analysis of bone mid-IR spectra provides useful information on bioapatite carbonate environments ( $\nu_2$  carbonate band at c. 850–900  $\text{cm}^{-1}$  and  $\nu_3$  carbonate mode at c. 1400–1600  $\text{cm}^{-1}$ ) and how they interact with calcite during recrystallization.

### Collagen

1. Collagen yields do not show any strong correlation with crystallinity suggesting that bioapatite recrystallization is possible even in the presence of reasonable amounts of collagen in bone.
2. The two human petrous bones display good collagen preservation, with about half of the initial collagen content surviving.
3. The Am/P ratio can potentially provide valuable information on the relative amount of collagen in bone, while GHI's use as collagen indicator is limited.
4. 2<sup>nd</sup> derivative analysis of the amide I band (c. 1600–1700  $\text{cm}^{-1}$ ) of bone mid-IR spectra can provide useful information on the components lost (e.g., polyproline II, cross-links) during collagen degradation.



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